## RHEOLOGICAL ANALYSIS OF CAPSULE SUSPENSIONS CONTAINING DIFFERENT SIZE CAPSULES

Hiroki Ito<sup>1,\*</sup>, Yohsuke Imai<sup>2</sup>, Daiki Matsunaga<sup>2</sup>, Toshihiro Omori<sup>1</sup>, Takami Yamaguchi<sup>1</sup> and Takuji Ishikawa<sup>2</sup>

 <sup>1</sup> Department of Biomedical Engineering, Tohoku University, 6-6-01, Aoba, Aramaki, Aoba-ku, Sendai 980-8579, Japan, ito@pfsl.mech.tohoku.ac.jp
<sup>2</sup> Department of Bioengineering and Robotics, Tohoku University, 6-6-01, Aoba, Aramaki, Aoba-ku, Sendai 980-8579, Japan,

vimai@pfsl.mech.tohoku.ac.jp

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A particle that has an inner fluid enclosed by a thin elastic membrane is called a capsule. This structure is found in red blood cells and polymer coated medicines. Many studies have been conducted to reveal the rheology of capsule suspensions for industrial and biomedical applications. In a real system, there is a size distribution of capsules with a capsule suspension. However, few studies have focused on the effect of such a size difference on the rheology of capsule suspensions. In this study, we numerically investigate suspensions containing capsules of two different sizes under simple shear flow.

We consider a capsule suspension under Stokes flow. We use a method developed by Matsunaga *et al.*[1], which applies GPU computing to a method coupling of the finite element method and boundary element method proposed by Walter *et al.*[2]. The membrane obeys the Skalak constitutive law, and bending moments in the membrane ignored. The capillary number  $Ca = \mu_f \dot{\gamma} a/G_s$  is a non-dimensional number which escribes the ratio between the viscous, and elastic forces where  $\mu_f$  is the viscosity of the fluid,  $\dot{\gamma}$ is the shear rate and  $G_s$  is the shear elastic modulus of the membrane. We fix Ca of large and small capsules as  $Ca_l = Ca_s = 1.0$ . Under a given volume fraction of capsules  $\phi$ , we change the ratio of small capsules to total capsules  $R_{\phi} = \phi_s/\phi$  or the radius ratio of a small capsule to a large capsule  $Ra = a_s/a_l$ . We show examples of the simulation in Figure 1. The apparent shear viscosity  $\eta$  can be described by  $\eta = \mu_f + \mu_p$ , where  $\mu_p = \sum_{12}^p / \dot{\gamma}$  is the increased viscosity due to the existence of capsules. Here,  $\sum_{ij}^p$  is the particle stress tensor, and can be expressed by

$$\Sigma_{ij}^{p} = \frac{1}{V} \sum_{n=1}^{N} \int_{A_{n}} \left\{ \frac{1}{2} \left( x_{i} q_{j} + q_{i} x_{j} \right) \right\} dA_{n}, \tag{1}$$

where V is the volume of the computational domain,  $x_i$  is a position coordinate,  $q_i$  is a point force, N is the number of capsules in the domain and  $A_n$  is the surface area of a capsule membrane.

Figure 2 shows  $\mu_p$  for Ra = 0.5 as a function of  $R_{\phi}$ , where  $\mu_p^{\text{ref}}$  is the value at  $R_{\phi} = 0.0$  and angle brackets denote the time-averaged value. Because Ca is the same for both large and small capsules, monomodal cases ( $R_{\phi} = 0.0, 1.0$ ) show the same value. On the other hand, in bimodal suspensions,  $\mu_p$  drops by a few percent, and this tendency becomes stronger at higher values of  $\phi$ . Figure 3 shows  $\mu_p$  as a function of Ra for  $R_{\phi} = 0.5$ . We found that the reduction of  $\mu_p$  in bimodal suspensions becomes larger when Ra is smaller; for example, it decreases by approximately 10% at Ra = 0.3.



Figure 1: The snapshots of the numerical result for  $\phi = 0.4$ . (a) $R_{\phi} = 0.0$ . (b) $R_{\phi} = 0.25$ . (c) $R_{\phi} = 0.5$ . The bright zone is the original computational domain.



Figure 2: The fluctuation component of the shear viscosity  $\mu_p$  as a function of  $R_{\phi}$ . Each value is normalized by the value at  $R_{\phi} = 0.0$ , and Ra is fixed at 0.5.



Figure 3: The fluctuation component of the shear viscosity  $\mu_p$  as a function of Ra. Each value is normalized by the value at Ra = 0.0, and  $R_{\phi}$  is fixed at 0.5.

## REFERENCES

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