A systematic comparison of 3D solid, shell and membrane formulations for the simulation of arterial wall mechanics

Miquel Aguirre^{*1,2}, Rogelio Ortigosa³, Nitesh Nama², Antonio J. Gil³ and C. Alberto Figueroa²

¹ Tecnalia Research & Innovation, Parque Tecnológico de Bizkaia, C/Geldo, Edificio 700 E-48160 Derio Bizkaia Spain, <u>miquel.aguirre@tecnalia.com</u>

² University of Michigan, North Campus Research Complex, 2800 Plymouth Road, Building 20 – 211W, Ann Arbor, MI 48109, {nnama,figueroc}@med.umich.edu

Sunding 20 - 211 w, Ann Arbor, Wi 46109, {<u>innania, rigueroc</u>}(<u>wined, uniter.cu</u>

³ Zienkiewicz Centre for Computational Engineering, College of Engineering Swansea University Bay Campus, Engineering Central, Swansea University

Fabian Way, Crymlyn Burrows, Swansea, SA1 8EN, Wales, UK {r.ortigosa,a.j.gil}@swansea.ac.uk

Key Words: Arterial wall mechanics, membrane, shell, incompressible

Computational modelling of arterial wall mechanics is now a key component in many areas of vascular disease research. The arterial wall can be modelled, with increasing degree of detail, as a membrane structure, a shell structure or a full three dimensional solid. Depending on the specific application, a choice must be made between these options, reaching a compromise between accuracy and computational cost. When it comes to deciding the optimal option, the decision relies mostly on intuition or previous experience, and is often unclear what the impact on numerical accuracy impact is.

This paper presents a systematic comparison between these three models, using in-house codes previously implemented for different applications. The first model is a nonlinear incompressible membrane model implemented within the software CRIMSON for FSI modelling of the vascular system [1]. The second is a rotationless incompressible shell model, enhanced with extra degrees of freedom (thickness stretch and the hydrostatic pressure), previously used in electromagnetics applications [2]. The third model is a low order three-dimensional model implemented within a Finite Element code for fully incompressible solids, using a new set of conservation laws for solid dynamics [3].

Different idealized geometries and constitutive models are used to compare the accuracy and efficiency of these approaches. Results are also compared to the close form given by an axisymmetric problem, either assuming thin or thick wall assumptions. A general guideline is provided to choose the adequate approach depending on the specific application and geometry.

REFERENCES

- [1] Khlebnikov, R., & Figueroa, C. A. (2015, October). Crimson: towards a software environment for patient-specific blood flow simulation for diagnosis and treatment. In Workshop on Clinical Image-Based Procedures (pp. 10-18). Springer, Cham.
- [2] Ortigosa, R., & Gil, A. J. (2017). A computational framework for incompressible electromechanics based on convex multi-variable strain energies for geometrically exact shell theory. Computer Methods in Applied Mechanics and Engineering, 317, 792-816.
- [3] Gil, A. J., Lee, C. H., Bonet, J., & Aguirre, M. (2014). A stabilised Petrov–Galerkin formulation for linear tetrahedral elements in compressible, nearly incompressible and truly incompressible fast dynamics. Computer Methods in Applied Mechanics and Engineering, 276, 659-690.